



Research Article

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Bond Strength Between A Hard Chairside Reline and A Printed Denture Base Compared to A Conventional Heat Polymerized Denture Base: An *In Vitro* Study

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Abstract

Introduction: The aim of this study was to test the shear and tensile bond strengths (MPa) of a hard chairside relined to a 3D printed denture base and compare it to a conventional heat polymerized denture base.

Material and methods: Sixty (n=15/test) blocks (70mm x 9mm x 9mm) of a printed polymethyl methacrylate (P-PMMA) (DENTCA 3D Printed Dentures) were provided by the manufacturer, while sixty (n=15 per test) blocks (70mm x 9mm x 9mm) of thermopolymerizable polymethyl methacrylate (T-PMMA) (Diamond D. Keystone) were prepared. Three millimeters of hard liner (Tokuso-Tokuyama America Inc.) was applied between two blocks. All the tests were conducted with an INSTRON Universal Testing machine.

Results: Statistically significant differences were found in the bond strength for the shear ($p < 0.003$) and the tensile ($p < 0.0001$) tests between the materials. In both instances, the bond strength of the hard liner with the P-PMMA was weaker compared to the T-PMMA with $6.22\text{MPa} \pm 0.78\text{SE}$ and $9.82\text{MPa} \pm 0.78\text{SE}$ respectively in the shear test, and $3.61\text{MPa} \pm 0.42\text{SE}$ and $6.68 \pm 0.42\text{SE}$ respectively in the tensile test. The force of rupture was also significantly lower in the P-PMMA $101.99\text{MPa} \pm 12.04\text{SE}$ versus the T-PMMA with $143.64\text{MPa} \pm 12.04\text{SE}$ during the shear test ($p < 0.021$) and the tensile test ($p < 0.0002$) with $360.96\text{MPa} \pm 41.97\text{SE}$ versus $611.18\text{MPa} \pm 41.97\text{SE}$ respectively.

Conclusion: In the context of this study, the bond between the hard liner and the printed polymethyl methacrylate was shown to be weaker when compared to the thermopolymerizable polymethyl methacrylate. Further investigation of the surface properties of CAD/CAM denture bases such as surface chemistry and the clinical impact of these results are suggested. As the use of CAD/CAM technology gains in popularity, more materials developed for traditional dentures should be studied for compatibility.

Keywords: CAD/CAM; Printed denture; Polymethyl methacrylate; Hard relined; Tensile bond strength; Shear bond strength

Abbreviations: CAD/CAM: Computer-aided design and computer-aided manufacturing; P-PMMA: Printed polymethyl methacrylate; T-PMMA: Thermopolymerizable polymethyl methacrylate; MPa: Megapascal; SE: Standard error

Introduction

Computer-aided design and computer-aided manufacturing (CAD/CAM) technology is increasingly used for different applications in dentistry such as fixed prostheses and more recently, removable dentures [1]. This is a promising avenue that could reduce the error accumulation in data collection and avoid the dimensional changes during the laboratory steps such as acrylic polymerization shrinkage, since the final product is printed or milled from prepolymerized blocks [2-4]. This newer approach is attractive for both clinicians and patients since it translates into two or three appointments completion, permits digital archiving, and demonstrates an improved denture base adaptation [1, 3, 5].

However, as the oral condition of patients evolves over time [6-7], continuous residual ridge resorption may lead to denture failure and consequently, the removable dentures will require adjustments regardless of the selected approach [8]. Several methods exist to adapt the removable prosthesis to the gradual changes in residual alveolar ridge contours, thus avoiding the continuous substitution, and relining is one of them. In this study, we are particularly interested in chairside hard relining, a practice that may be indicated when a lack of retention, due to missing material (acrylic), is present in patients with stable oral conditions and no expected significant changes. If a denture was prepared with CAD/

CAM technology and relining was required, it would be crucial to ensure that the existing relining materials are compatible and can adequately be bonded to the denture base.

This study compares the shear and tensile bond strengths of a hard chairside reline material [9] (Tokuso-Tokuyama America Inc.) with printed polymethyl methacrylate (P-PMMA) (DENTCA 3D Printed Dentures) as used in the fabrication of prostheses with the CAD/CAM technique versus strength of the same relining material with the thermopolymerizable polymethyl methacrylate (T-PMMA) (Diamond D. Keystone) as used in the fabrication of prostheses with the conventional technique.

Materials and Methods

Preparation of the specimens

Sixty blocks of P-PMMA (70mm x 9mm x 9mm) were provided by DENTCA 3D Printed Dentures. Sixty blocks of T-PMMA (Diamond D. - Keystone Industries, USA) of equal dimensions to the P-PMMA blocks were prepared using the conventional method with the lost wax technique in a denture flask (Hanau, Whip Mix, USA) (Figure 1). The flasks were polymerized overnight according to the manufacturer's recommendations in a 165°F water bath for 10 hours.



Figure 1: Plaster mold in brass denture flask produced for the conventional acrylic lost wax technique.

The work surface of each block was unpolished with a carbide bur (H72E.11.060, Brasseler, USA). The adhesive was applied, and pairs of blocks were stabilized at 3mm distance from each other (Figure 2). The autopolymerizing hard denture liner (Tokuso-Tokuyama America Inc.) was prepared according to the

manufacturer's recommendations which is composed of a polyethyl methacrylate acrylic (PEMA) powder and a β -methacryloyl oxyethyl propionate (MAOP) liquid. The relining material was then injected with a syringe between the two work surfaces and compacted with a spatula.

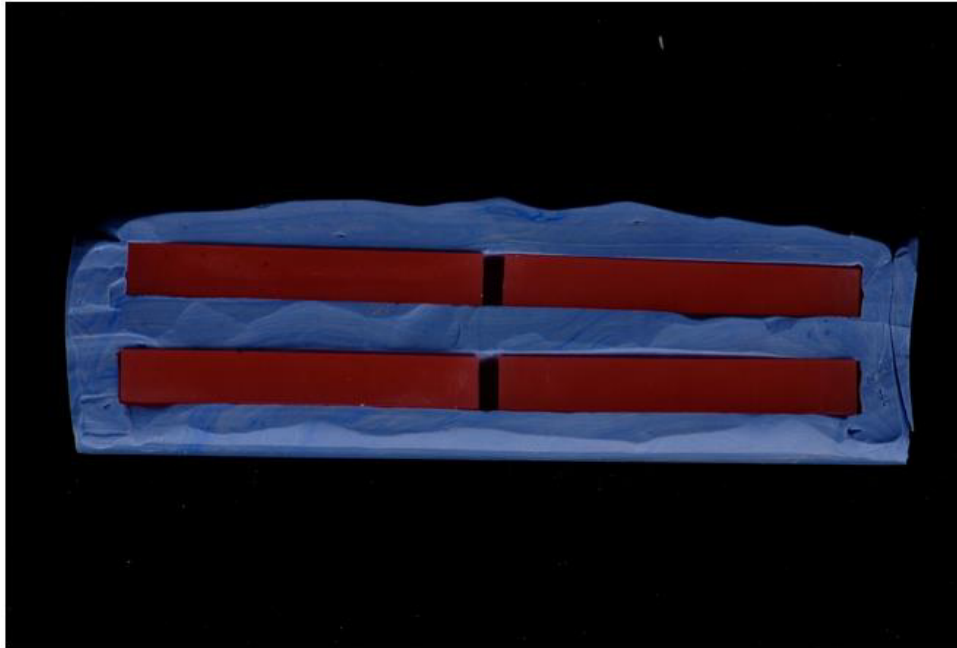


Figure 2: Pairs of blocks stabilized at 3 mm distance from each other for relining material injection.

A total of sixty specimens were prepared and divided into four groups of 15 specimens each (Table 1). Each specimen is composed of two blocks of the same material (Figure 3). All the tests were

conducted with an INSTRON Universal Testing machine (Model 5944, Instron Corporation, Norwood, MA, USA).



Figure 3: Representative specimen (P-PMMA).

Table 1: Test groups.

Group	Material	Size	Test
1	T-PMMA	n=15	Shear Shear
2	P-PMMA	n=15	
3	T-PMMA	n=15	Tensile Tensile
4	P-PMMA	n=15	

Abbreviations: P-PMMA: Printed polymethyl methacrylate;
T-PMMA: Thermopolymerizable polymethyl methacrylate.

Shear stress and tensile strength tests

For the shear stress test, the uniaxial force was applied vertically from the top on a horizontally placed specimen, at 1cm distance from the fixed section, with a head speed of 1mm/min until failure (Figure 4). Load and extension, in Newton and mm respectively, were recorded with an acquisition rate of 100ms. For the tensile strength test, the uniaxial force was applied vertically from the top on a vertically mounted specimen with a head speed of 5mm/min until failure (Figure 5). Load and extension, in Newton and mm respectively, were recorded with an acquisition rate of 100ms.



Figure 4: Shear stress test setup with specimen (T-PMMA) in horizontal position.



Figure 5: Tensile strength test setup with the specimen (P-PMMA) in vertical position.

Fracture analysis

For all the tested specimens, the fracture was considered adhesive when failure occurred between the relining material and the acrylic resin, cohesive when a fracture was inside the relining material, or mixed when both occurrences were observed in the same fracture. The mode of fracture was determined visually.

Statistical analysis

The statistical package SAS software, version 9.4 (SAS Institute Inc., Cary NC) was used for all the analyzed data with respect to the different tests. The average tensile and shear strengths and standard deviation (SD) were calculated for each group. Student's T test was used to analyze the statistical difference among the tested groups with a power of 80% and a significance threshold of 5%.

Results

Shear stress test

For shear bond strength, P-PMMA specimens exhibited significantly lower ($p < 0.003$) mean values compared to the conventional specimens with a mean and standard error of $6.22\text{MPa} \pm 0.78\text{SE}$ versus $9.82\text{MPa} \pm 0.78\text{SE}$ from the T-PMMA specimens (Table 2). The force at rupture of P-PMMA specimens were also significantly lower ($p < 0.02$) than those of the T-PMMA specimens with $143.64\text{MPa} \pm 12.04\text{SE}$ and $101.99\text{MPa} \pm 12.04\text{SE}$ respectively (Table 3). Fisher's Exact test was used to compare the proportion of fractures of each type according to the group. There was a significant difference ($p < 0.006$) with 100% adhesive fracture rate for the P-PMMA method against 53% in the T-PMMA (Table 4) where the rest was mixed.

Table 2: Shear bond strength of specimens.

Shear Bond Strength							
Group	Estimate (MPa)	Standard Error	DF	t Value	Pr > F	Lower	Upper
CAD/CAM	6.218	0.7832	28	7.94	0.003	4.6137	7.8223
Conventional	9.8213	0.7832	28	12.54		8.2171	11.4256

Abbreviation: DF: Degrees of freedom.

Table 3: Force of rupture of specimens for shear test.

Force of Rupture for the Shear Test							
Group	Estimate (MPa)	Standard Error	DF	t Value	Pr > F	Lower	Upper
CAD/CAM	101.99	12.0431	28	8.47	0.021	77.3196	126.66
Conventional	143.64	12.0431	28	11.93		118.97	168.31

Abbreviation: DF: Degrees of freedom.

Table 4: Type of fracture of specimens for shear test.

Table of Groups by Type of Fracture for Tensile Test					
Group		Type of fracture			
		Adhesive	Mixed	Cohesive	Total
CAD/CAM	Frequency	15	0	0	15
	Row Pct	100	0	0	
Conventional	Frequency	8	7	0	15
	Row Pct	53.33	46.47	0	
Total		23	7	0	30

Abbreviation: Pct: Percentage.

Tensile stress test

For the tensile bond strength, the adhesive strength of P-PMMA was found to be significantly lower ($p < 0.0001$) than that of the T-PMMA with $3.61\text{MPa} \pm 0.42\text{SE}$ and $6.68 \pm 0.42\text{SE}$ respectively (Table 5). The breaking force of the P-PMMA specimens were

significantly lower ($p < 0.0002$) than those of the T-PMMA with $360.96\text{MPa} \pm 41.97\text{SE}$ versus $611.18\text{MPa} \pm 41.97\text{SE}$ respectively (Table 6). The Fisher analysis was not done for the fractures caused by tensile stress, since all the fractures in both trial groups were adhesive (Table 7).

Table 5: Tensile bond strength of specimens.

Tensile Bond Strength							
Group	Estimate (MPa)	Standard Error	DF	t Value	Pr > F	Lower	Upper
CAD/CAM	3.6053	0.4243	28	8.5	<.0001	2.7361	4.4746
Conventional	6.6833	0.4243	28	15.75		5.8141	7.5526

Abbreviation: DF: Degrees of freedom.

Table 6: Force of rupture for tensile test.

Force of Rupture for the Tensile Test							
Group	Estimate	Standard Error	DF	t Value	Pr > F	Lower	Upper
CAD/CAM	360.96	41.9712	28	8.6	0.0002	274.99	446.93
Conventional	611.18	41.9712	28	14.56		525.21	697.16

Abbreviation: DF: Degrees of freedom

Table 7: Type of fracture of specimens for tensile test.

Table of Groups by Type of Fracture for Tensile Test					
Group		Type of fracture			
		Adhesive	Mixed	Cohesive	Total
CAD/CAM	Frequency	15	0	0	15
	Row Pct	100	0	0	
Conventional	Frequency	15	0	0	15
	Row Pct	100	0	0	
Total		30	0	0	30

Abbreviation: Pct: Percentage.

Discussion

The bond strength between a denture base and its relining material is used to indicate the durability and failure rate of the liner [10]. Shear and tensile stress tests are common strategies for the evaluation of the bond between denture bases and liners in literature [8, 11-14], and thus chosen for this study. The bonding between the liner and denture base is mainly provided by the diffusion, the penetration, and the polymerization of the reline monomers across the interface, thus forming interpenetrating polymer networks [15]. A recent study indicates a reduction of monomer content on the surface of CAD/CAM denture bases due to its method of preparation [16]. It is the same release of residual methyl methacrylate monomer (MMA) that affects the dimensional stability of conventional dentures. Although this presents many advantages clinically, like restrict polymerization shrinkage, enhanced mechanical properties, and decrease surface deterioration, it can also create a weaker bond when the application of a relining material is needed, since the interpenetration will not be optimal. However, this still requires more investigation. As surface finishing, chemical composition, topography, and roughness have been suggested to influence the adhesion between the acrylic and the relining material [17], the surface properties of the selected acrylics could explain the lower shear and tensile bond strengths of the CAD/CAM samples compared to the conventional ones [15, 18, 19]. In order to validate this hypothesis, a surface analysis should be included in future studies including the use of X-ray Photoelectron Spectroscopy (XPS) [20] for the surface chemical composition and Atomic Force Microscopy (AFM) [21] for the surface topography and roughness.

Since this study is preliminary, the used methodology lacks in recreating the patient's mouth environment. To conduct the tests in a physiologically relevant ambient, part of the samples could be subjected to water immersion or thermocycling to stimulate water aging [8] and the results could then be compared to untreated control samples. Immersion of resin liners in water results in water absorption between the polymeric chains, which forces them apart and decreases bonding between the surfaces, thus providing more clinically accurate results [13, 22, 23].

Conclusion

Within the limitations of this *in vitro* study, our results suggest that the bond between the printed polymethyl methacrylate denture base and the hard liner is weaker when compared to the bond of thermopolymerizable polymethyl methacrylate denture base and the hard liner. More research is needed to study the properties of CAD/CAM denture bases (such as surface finishing, chemical composition, topography, and roughness) and to understand the clinical impact of these results.

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Conflict of Interest

No Conflict of Interest.

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