



Surface Treatments of Titanium and Zirconia Implants: Impact on Bacterial Adhesion (Systematic Revue of Literature)

Moudni S^{1*}, Moussaoui H¹, Rochd T², Boujoual I¹ and Andoh A²

¹Fixed Prosthesis Department, Faculty of Dentistry of Casablanca, Hassan II University of Casablanca, Casablanca, Morocco

²Rochd T, Biology and fundamentals department, Faculty of Dentistry of Casablanca, Hassan II University of Casablanca, Morocco

*Corresponding author: Moudni S, Fixed Prosthesis Department, Faculty of Dentistry of Casablanca, Hassan II University of Casablanca, Casablanca, Morocco.

Received Date: May 09, 2022

Published Date: May 20, 2022

Introduction

The use of dental implants to restore the loss of one or many teeth has become a widely used treatment option in daily practice. However, as soon as implant surfaces or their components are exposed to human oral cavity, they are immediately covered by an acquired film and instantly subjected to bacterial colonization. This is directly influenced by the surface properties of the materials, including chemical composition, surface roughness, surface energy... [1]. In modern biomaterial research, implant surfaces are primarily modified to increase bone integration into the alveolar bone. Recently, implant surfaces are also modified to reduce biofilm formation after exposure to the oral cavity [2]. Currently, many implant systems with different surface treatments are available on the market, which makes it difficult for the practitioner to choose.

There are two main categories of implant surface treatments [3]:

-Either by adding substance: this is the addition treatment.

-or by altering the smooth surface: this is the subtraction treatment.

The main objective of this systematic review was to evaluate the impact of different surface treatments of titanium and zirconium implants on bacterial adhesion. The secondary objective was to compare bacterial adhesion on titanium and on zirconium implants.

Material and Methods

Research strategy

Three computer databases were used for the literature search: Pubmed, Cochrane, and Science Direct.

The search was conducted between 01/ 01/ 2011 and 01/ 02/ 2022. The review included well-conducted in vivo and/or in vitro trials and randomized trials written in English, evaluating the surface condition of titanium and zirconium dental implants and its relationship with bacterial adhesion. Exclusion criteria were case reports, systematic reviews of the literature, meta-analyses, literature reviews, animal and cadaver studies, and articles dealing with bacterial adhesion on supra-implant prosthesis.

The table below represents the keywords used in the different boolean equations and for each database (Table 1).

Table 1: keywords and boolean equations.

Databases	Boolean equations	Results
Cochrane	- Dental implant and bacteria	51 articles
Pubmed	- ("Dental Implants"[Mesh]) AND "Biofilms"[Mesh]	11 articles
	- ("Dental Implants"[Mesh]) AND "Bacteria"[Mesh]	26 articles
	- ("Dental Implants"[Mesh]) AND "Decontamination"[Mesh]	7 articles
	- ("Dental Implants"[Mesh]) AND "Anti-Infective Agents"[Mesh]	38 articles
	- ("Dental Implants, Single-Tooth"[Mesh]) AND "Surface Properties"	16 articles
Science Direct	- Dental implant - bacterial adhesion - titanium - zirconium	21 articles
	- Dental implant- surface treatment- bacterial adhesion	74 articles

Assessment of methodological quality

Two reviewers (M.S. & B.I.) assessed the methodological quality of the studies selected for analysis. This assessment was based on the tool "The Critical Skills Appraisal Program" (CASP) which was created from guides produced by the Evidence Based Medicine Working Group and published in the Journal of the American Medical Association [4].

Data extraction

To prepare and structure our systematic review, the focused question was developed using the PICO criteria:

P: Participants => Titanium and zirconium dental implants

I: Intervention => Implants with different surface treatments (by addition/subtraction) placed in contact with different bacteria.

C: Comparison => Control group (titanium or zirconium discs without surface treatment)

O: Outcomes => Relationship between the surface

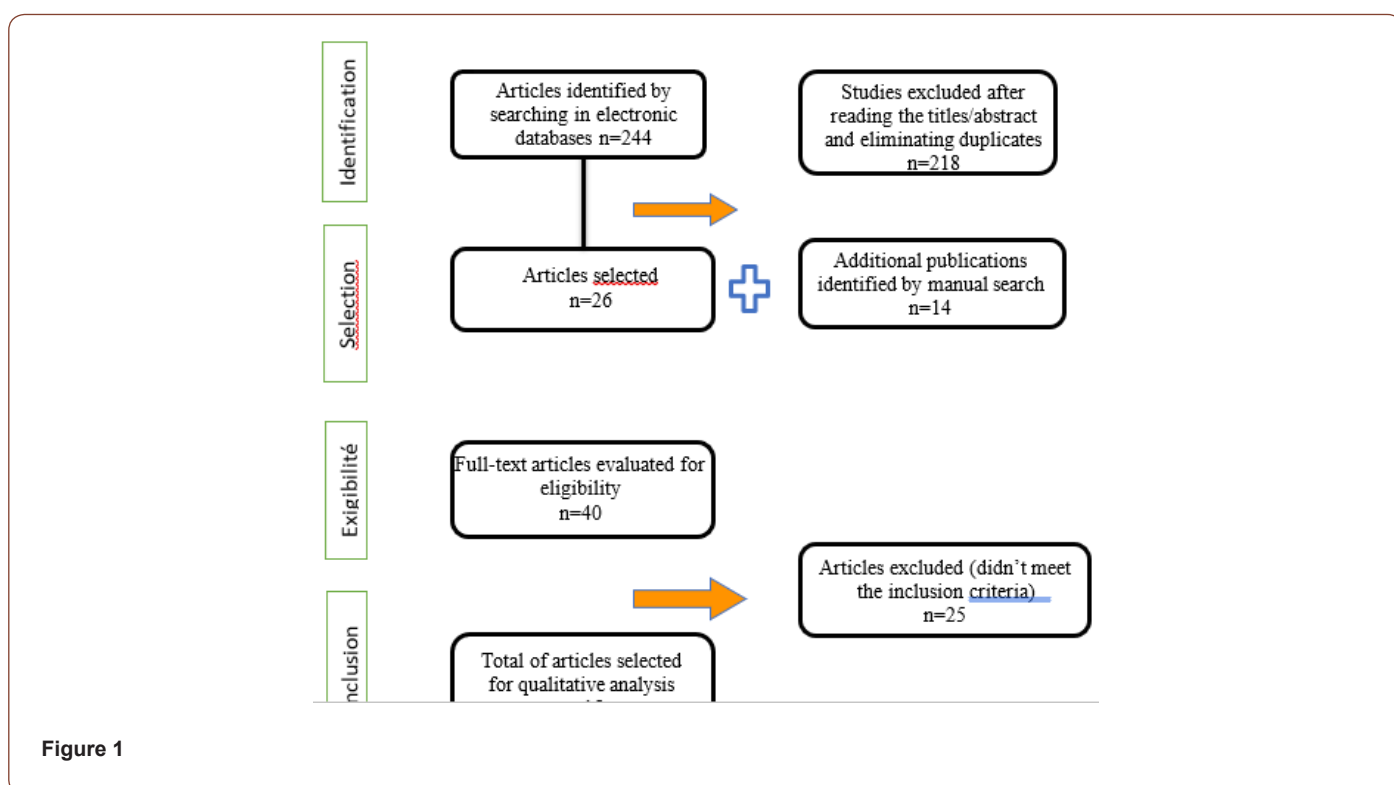
characteristics/the material of the implants and bacterial adhesion.

Data extraction was completed by 2 readers independently, with formal processes for discussion and consensus building in case of disagreement to minimize subjectivity during the multiple stages of completion.

The writing of this systematic review followed the PRISMA Statement "Preferred Reporting Items for Systematic reviews and Meta-Analyses" Moher, et al. [5].

Results

The search of the three databases identified a total of 244 studies from the automated search, from which we retained 26 studies after the first selection based on the reading of titles and abstracts and after eliminating duplicates. Through the manual search, we were able to group 14 articles. Thus, we had a total of 40 articles from which 25 articles were eliminated after applying the inclusion and exclusion criteria, resulting in the selection of 15 articles included in our review (Figure 1).

**Figure 1**

The 15 selected studies include 11 in vitro studies, 2 studies conducted in vivo and 2 studies conducted in vitro and in vivo. They were all performed using titanium or zirconium discs with different surface characteristics. The control group was constituted of titanium or zirconium discs without surface treatment. In vivo studies were performed with intra-oral splints with different discs for each tested sample.

Of the 15 studies included in our review, 10 investigated bacterial adhesion only on titanium discs. The other 5 studies included, in addition to titanium discs, zirconium discs with

different surface treatments.

The different parameters measured were essentially surface roughness of the material, its wettability through the measurement of the contact angle, chemical composition of the surfaces and analysis and quantification of the bacteria adhesion to the different surfaces after bacterial culture.

The different surface treatments used were multiple and heterogeneous and were classified into implant surface modification by addition or subtraction (Table 1) (Table 2).

Table 2: Classification of surface implant modifications used in the included studies.

Implant surface modification by addition	Implant surface modification by subtraction
<ul style="list-style-type: none"> -Implant grafted with silver by anodic spark deposition. -Implant grafted with gallium by anodic spark deposition. -Anodic oxidation of titanium. -calcium phosphate deposit on zirconia -Non-thermal atmospheric pressure plasma treatment 	<ul style="list-style-type: none"> -Sand-blasted and acid-etched surface treatment. -Sand-blasted surface treatment. -Acid-etched surface treatment. -Laser surface treatment.

Informations about the characteristics of these studies are presented in (Tables 3, 4), including a brief description of the

studies and their conclusions and the quality assessment of included studies is summarized in (Table 5).

Table 3: Bacterial adhesion and implant surface modification by addition.

Authors/ Year/ Type of the study	Patients/Samples/ Type	Studied bacteria	Studied parameters	Comparison	Conclusion
Lee, et al. [13] 2019 In Vitro	<ul style="list-style-type: none"> - Polished titanium disks - Plasma treated disks using compressed air gas. 	<ul style="list-style-type: none"> -S. mutans - S. aureus -K. oxyta -K. pneumoniae 	<ul style="list-style-type: none"> - Surface roughness. - Contact angle. - Chemical composition. - Bacterial adhesion. 	Between disks with and without treatment.	The plasma treatment caused a large increase in surface wettability without change in roughness and had a significant impact in decreasing the adhesion rate of bacteria.
Lee, et al. [14] 2016 In vitro	<ul style="list-style-type: none"> - Polished titanium disks. - Plasma treated disks using compressed air, ammonia and nitrogen gases. 	S. sanguinis	<ul style="list-style-type: none"> - Surface roughness. - Chemical composition. - Bacterial adhesion. - Cells viability. 	<ul style="list-style-type: none"> - Between disks with and without treatment. - Between the three gases 	<ul style="list-style-type: none"> - Plasma treatment caused an increase in surface wettability without change in roughness and had a significant impact in reducing the number of adherent bacteria on treated surfaces compared to untreated titanium. - The greatest reduction of bacteria was observed with the nitrogen treatment.
Cochis, et al. [10]. 2014 In vitro et in vivo	<ul style="list-style-type: none"> - 7 patients. - Titanium disks without treatment. - Disks modified by anodic spark deposition. 	S. mutans	<ul style="list-style-type: none"> - Evaluation of the metabolic state of the cells. - Antibacterial activity. - Surface morphology. - Biofilm thickness. - Cytocompatibility. 	<ul style="list-style-type: none"> - Between disks with and without treatment. - Between silver and gallium deposition. 	Significant decrease in viability and number of bacteria on treated surfaces compared to untreated ones, with no cytotoxicity in relation to gallium nitrate and silver nitrate.

Della Valle, et al. 2012 [11] In vitro	- Disks modified by silver anodic spark deposition - Non-treated titanium disks.	- E. coli - S. epidermidis - S. mutans	- Surface characterization. - Surface morphology and chemical composition. - Surface roughness - Cells viability. - Bacterial adhesion.	-Between disks with and without treatment.	- Surfaces treated with silver particle deposition had a positive effect on osteoblast adhesion and spreading. - Increased surface roughness and significantly reduced bacterial adhesion on treated samples compared to untreated ones.
Lorenzetti, et al. 2015 [19] In vitro	- Titanium disks modified by hydrothermal treatment to synthesize nanostructured TiO ₂ -anatase coatings. (Anodisation) - Non-treated titanium disks.	E. coli	- Surface morphology. - Surface topography. - Contact angle. - Bacterial adhesion.	- Between disks with and without treatment.	- Significant increase in surface roughness and wettability after titanium treatment. - Significant reduction in the number of adherent bacteria on treated surfaces compared to untreated ones.
Pantaroto, et al. 2017 [17] In vitro	- Titanium disks modified by radiofrequency (RF) magnetron sputtering treatment to obtain TiO ₂ films composed of anatase (A-TiO ₂), rutile (R-TiO ₂) or mixture of crystalline structures (anatase + rutile) (M-TiO ₂) - Non-treated titanium disks.	-S. sanguinis - A. naelundii - F. nucleatum	-Surface morphology. -TiO ₂ film thickness. -Surface free energy. - Bacterial adhesion.	- Between disks with and without treatment. - Between the crystalline structures. - Bacterial adhesion before and after UV irradiation.	- Titanium with TiO ₂ coating in anatase phase showed the highest value of surface roughness and surface contact angle (Ra=0.11µm et CA= 90°). - Significant decrease in the number of adherent bacteria on the anatase and mixed crystalline structures, while there was no antibacterial effect on the rutile crystalline structure.
Al Ahmad, et al. 2013 [20] In vivo	- 6 healthy patients. - Machined titanium - Machined zirconia - Modified titanium by anodic oxydation - Modified zirconia by calcium phosphate deposition. -Bovine enamel slabs.	Salivary bacteria	- Wearing an intraoral splint with 6 different implant materials and an enamel plate for 30 and 120 minutes. - Bacterial adhesion.	- Between titanium and zirconium disks with and without treatment. - Between the different surface treatments. - Between titanium and zirconium.	-Surface roughness had a significant impact in increasing the number of adherent bacteria on titanium and zirconium surfaces. -Streptococcus spp. represents the largest proportion of bacteria on the different tested surfaces after the 2 exposure times.

Table 4: Bacterial adhesion and implant surface modification by subtraction.

Authors/ Year/ Type of the study	Patients/ Samples/ Type	Studied bacteria	Studied parameters	Comparison	Conclusion
Bevilacqua, et al. 2018 [16] In vitro et In vivo	- 3 healthy patients aged between 21 and 25 years old. - Machined titanium - Laser treated titanium (LT) - Sandblasted titanium	- Pseudomona aeruginosa - Salivary bacteria	- Biofilm quantity and thickness.	- Between disks with and without treatment. - Between laser treated titanium and sanblasted one.	In Vivo: After 1 day: - Machined Ti: Bacteria were more numerous. - Average biofilm thickness was almost equal on all surfaces. After 4 days: - No significant difference in biofilm thickness and amount on different surfaces. (p>0.05) In Vitro: - Machined surfaces are less likely to allow bacterial growth than other surfaces. - LT surfaces allowed 22% less biomass than sandblasted surfaces.

Ribeiro, et al. 2016 [21] In vivo	<ul style="list-style-type: none"> - 10 healthy patients. - 10 machined titanium (Ti-M) - 10 acid-etched treated titanium (Ti-AE) - 10 laser treated titanium (LT) 	<ul style="list-style-type: none"> - S. oralis - Other oral bacteria 	<ul style="list-style-type: none"> - Surface morphology. - Bacterial adhesion. 	<ul style="list-style-type: none"> - Between disks with and without treatment. - Between laser treated titanium and acid-etched one. 	<ul style="list-style-type: none"> - Significant increase in roughness of Ti-AL compared to Ti-AE and Ti-M.(p<0.05) Ti-M: long alternating grooves with flat surfaces. Ti-AE: rough micro-structure with open pores on the whole surface. Ti-AL: more dispersed and rounded micropores than Ti-AE. - Similar level of bacterial adhesion on the 3 surfaces in terms of quantity of adherent bacteria and quantity of S. oralis.
Drago, et al. 2016 [22] In vitro	<ul style="list-style-type: none"> - Laser treated titanium (LT) - Sandblasted titanium (SB) 	<ul style="list-style-type: none"> -Staphylococcus aureus - Pseudomonas aeruginosa -Porphyromonas gingivalis 	<ul style="list-style-type: none"> - Surface morphology. - Bacterial adhesion. - Cell viability 	<ul style="list-style-type: none"> - Between laser treated titanium and sanblasted one. 	<ul style="list-style-type: none"> - Laser surface treatment causes a significant decrease in the number of adherent bacteria. - Laser treatment interferes with the ability of bacteria to adhere to the titanium surface.
Torsten, et al. 2016 [8] In vitro	<ul style="list-style-type: none"> - 20 titanium disks - 20 zirconium disks - Polished titanium and zirconium disks. - Sandblasted titanium and zirconium disks with alumina of 50 or 250µm. -Titanium and zirconia discs treated by application of an n-propylsilane to modify the surface energy of the specimens and modification of hydrophilic conditions by application of an amino-silane. 	<ul style="list-style-type: none"> - S. sanguinis - S. epidermidis 	<ul style="list-style-type: none"> - Surface roughness - Surface free energy - Bacterial adhesion 	<ul style="list-style-type: none"> - Between disks with and without treatment. -Between titanium and zirconium disks. - Between the different surface treatments. 	<ul style="list-style-type: none"> - Sandblasting significantly increased the surface roughness value of both titanium and zirconium. This increase was greater on titanium. - The adhesion of S. sanguinis was significantly higher on ceramic surfaces than on titanium surfaces (p<0.05).
Zhao, et al. 2014 [9] In vitro	<p>Titanium and zirconia discs treated by:</p> <ol style="list-style-type: none"> 1- polishing (P), 2- grinding (M), 3- grinding then etching in a boiling mixture of concentrated HCl and H₂SO₄ (or hydrofluoric acid in case of ZrO₂) then rinsing (MA) 4- grinding and etching with HCl/H₂SO₄ 	<ul style="list-style-type: none"> - S. mitis - S. oralis - S. salivarius HB - S. aureus 	<ul style="list-style-type: none"> - Contact angle. - Surface roughness. - Bacterial adhesion. 	<ul style="list-style-type: none"> - Between disks with and without treatment. -Between titanium and zirconium disks. - Between the different surface treatments. 	<ul style="list-style-type: none"> -Etching significantly increased the surface roughness of both titanium and zirconia. -Zirconia attracts biofilm more than titanium.

Roehling, et al. 2016 [23] In vitro	Titanium disks: -Machined (TiM) - SLA (sandblasted and acid-etched) Zirconium disks: -Machined (ZiM) - ZLA (sandblasted and acid-etched)	- P. gingivalis - F. nucleatum - S. sanguinis	-Biofilm structure. - Biofilm thickness. - Free energy - Biofilm metabolism.	- Between disks with and without treatment. - Between titanium and zirconium disks. - Between SLA and ZLA.	- Bacterial adhesion on SLA was greater than on machined titanium. - Biofilm formation on zirconia showed a significant reduction compared to titanium.
Hauslich, et al. 2011 [7] In vitro	Titanium disks: -Machined (TiM) - Acid-etched (Ti-AE) - SLA (sandblasted and acid-etched)	- P. gingivalis - F. nucleatum - S. mutans	- Bacterial adhesion.	- Between disks with and without treatment. - Between acid-etched titanium and SLA.	-Bacterial adhesion is dependent on the surface roughness of the material. -Removal of Ca++ from the surface caused a significant decrease in bacterial adhesion.
Chen, et al. 2016 [24] In vitro	Titanium disks: -Machined (TiM) - Sandblasted (Ti-SB) - SLA (sandblasted and acid-etched)	E. coli	- Contact angle. - Surface roughness. - Surface morphology. - Bacterial adhesion.	- Between disks with and without treatment. - Between sandblasted titanium and SLA.	-Surface roughness is not a determining parameter in bacterial adhesion. -Bacterial adhesion on sandblasted titanium is not significantly different from that on SLA surfaces.

Table 5: Assessment of methodological quality of the included studies.

Etudes	Q1	Q2	Q3	Q4	Q5	Q6	Q7	Q8	Q9	Q10	Q11	Q12	Total
Cochis, et al. 2014 [10]	Yes	Yes	Yes	Yes	No	No	Yes	Yes	Yes	Yes	Yes	Yes	10
Zhao, et al. 2014 [9]	Yes	Yes	Yes	Yes	No	No	Yes	Yes	Yes	No	Yes	Yes	9
Al Ahmad, et al. 2013 [20]	Yes	Yes	Yes	Yes	No	No	Yes	Yes	Yes	Yes	Yes	Yes	10
Ribeiro, et al. 2016 [21]	Yes	Yes	Yes	Yes	No	No	Yes	Yes	Yes	Yes	Yes	Yes	10
Lee, et al. 2016 [14]	Yes	Yes	Yes	Yes	No	No	Yes	Yes	Yes	No	Yes	Yes	9
Lee, et al. 2019 [13]	Yes	Yes	Yes	Yes	No	No	Yes	Yes	Yes	No	Yes	Yes	9
Torsten, et al. 2016 [8]	Yes	Yes	Yes	Yes	No	No	Yes	Yes	Yes	No	Yes	Yes	9
Bevilacqua, et al. 2018 [16]	Yes	Yes	Yes	Yes	No	No	Yes	Yes	Yes	Yes	Yes	Yes	10
Chen, et al. 2016 [24]	Yes	Yes	Yes	Yes	No	No	Yes	Yes	Yes	No	Yes	Yes	9
Hauslich, et al. 2011 [7]	Yes	Yes	Yes	Yes	No	No	Yes	Yes	Yes	No	Yes	Yes	9
Roehling, et al. 2016 [23]	Yes	Yes	Yes	Yes	No	No	Yes	Yes	Yes	No	Yes	Yes	9
Drago, et al. 2016 [22]	Yes	Yes	Yes	Yes	No	No	Yes	Yes	Yes	No	Yes	Yes	9
Della Valle, et al. 2012 [11]	Yes	Yes	Yes	Yes	No	No	Yes	Yes	Yes	No	Yes	Yes	9
Lorenzetti, et al. 2015 [19]	Yes	Yes	Yes	Yes	No	No	Yes	Yes	Yes	No	Yes	Yes	9
Pantaroto, et al. 2017 [17]	Yes	Yes	Yes	Yes	No	No	Yes	Yes	Yes	No	Yes	Yes	9

Discussion

This work focused on the effect of different surface treatments of titanium and zirconium dental implants on bacterial adhesion. This question was addressed by in vitro and/or in vivo studies. Several parameters are involved in the phenomenon of bacterial

adhesion on dental implants. Surface roughness is a widely evaluated parameter. According to Wennerberg, et al. [6], dental implant surfaces are classified into four different groups based on their roughness: smooth surfaces ($Ra < 0.5 \mu m$), minimally rough surfaces ($0.5 < Ra < 1.0 \mu m$), moderately rough surfaces ($1.0 < Ra < 2.0 \mu m$), and rough surfaces ($Ra > 2.0 \mu m$).

According to Hauslich, et al. [7], increasing surface roughness increases bacterial adhesion to implant surfaces. However, other studies [12-20] have shown that surface roughness only affects the early stage of biofilm development. Torsten and Zhao [8, 9], on the other hand, have shown that roughness is not the only determinant of bacterial adhesion. Three-dimensional analyses of the microstructure are necessary [8]. Considering the studies carried out in vivo and in vitro using complex bacterial communities close to the oral context where the bacterial flora is rich and varied, it was concluded that the surface roughness intervenes only during the initial bacterial attachment.

Furthermore, the use of surface treatment by electro-deposition of silver or gallium showed a great decrease in bacterial adhesion on the surfaces despite the increase in surface roughness [10, 11]. This was explained by the fact that silver nanoparticles in the microporous titanium oxide layer are readily available to react with water and release silver ions. These later are known to bind strongly to electron donor groups in biological molecules containing sulfur, oxygen or nitrogen causing defects in the bacteria cell wall so that cell contents are lost. In addition, silver ions bound to proteins can alter bacterial cells metabolism and change membrane permeability and respiration. Both of these effects lead to bacterial cell death [9]. According to Wennerberg and Albrektsson [12], there is an optimal surface roughness window of 1 to 1.5 μ m. They consider that a higher value leads to a loss of bone anchorage. They add that it is very difficult to compare different studies, especially because the techniques used for characterization of surface topography vary considerably.

The surface energy of implant materials is also an important parameter influencing bacterial adhesion. Hydrophilic surfaces prevent bacterial attachment and can be achieved by increasing the wettability. The treatment of implant surfaces with plasma had led to significant increase in surface energy of titanium (4x more than untreated one), and consequently, to a significant reduction in the number of adherent bacteria [13, 14]. This was explained by the fact that bacteria with hydrophobic properties prefer hydrophobic surfaces and tend not to attach to hydrophilic surfaces and vice versa. However, the majority of bacteria involved in peri-implantitis are hydrophobic species. These results are in agreement with a review of literature about the wettability of dental implant surfaces, which concluded that among the benefits of hydrophilic surfaces is the reduction of adhesion of bacteria such as *Staphylococcus aureus*, *Streptococcus sanguinis*, and *Staphylococcus epidermidis* [15].

Concerning the crystalline phase of the surface, titanium dioxide can be found in three crystalline structures: anatase, rutile and brookite. These have a photocatalytic activity responsible for their anti-bacterial properties. The different structures can be generated by different methods like anodic oxidation, hydro-thermal treatment and plasma treatment. TiO₂-anatase coatings, which were previously proven to improve corrosion resistance, affect the plasma protein adsorption and enhance osteogenesis, have also shown strong antibacterial activity on titanium surfaces [16]. This can be attributed to the presence of anatase phase and its large band gap (3.2 eV) promoting high energy to create electrons

and holes, and consequently to form more reactive oxygen species, when compared to rutile [17].

With regard to the implant material, titanium is the most frequently used reference material because of its biocompatibility and excellent mechanical properties. Recently, high-strength zirconia (ZrO₂) implants have been invented as an alternative to titanium implants because of their resistance to corrosion and their enhanced aesthetics in case of exposure. Bacterial adhesion on titanium and zirconia does not seem to show any significant difference. Titanium is coated by a layer of surface oxide, which physical and mechanical characteristics are more closely related to ceramic than to metal. This phenomenon may explain why similar protein-binding properties on titanium and zirconium oxide have been reported and why zirconia did not show any reduced bacterial adhesion [8]. A randomized clinical trial, performed in vivo and in vitro, revealed no significant difference in the colonized surface area in the different discs ($p=0.0730$) as well as a high percentage of coverage by biofilm on all materials tested (90.9% of the total surface area of zirconia and 84.14% on machined titanium) [18]. Nevertheless, the number of studies on bacterial adhesion on zirconia remains very low, and other studies should be carried out on a larger number of patients to confirm the experimental results found [19-24].

Conclusion

Based on the results of this systematic review, the following conclusions can be drawn:

- Roughness is only involved in the early stage of biofilm development and not in its maturation.

- Increasing the wettability of materials by creating hydrophilic surfaces has shown very good results in reducing the number of bacteria adhering to them.

- The use of materials in anatase crystalline structure has proven to be an important factor in the development of an antimicrobial surface.

- The deposition of a thin layer of silver nanoparticles may be an option to provide the implant with anti-bacterial characteristics on its surface and contribute to the prevention of peri-implant inflammatory processes. However, it is essential that the particles are securely fixed to prevent their entrance to the circulation.

- As for adhesion on zirconia and titanium, the results of the majority of studies have shown no difference in bacterial colonization between the two. However, further clinical investigations are still needed.

Acknowledgment

None.

Conflict of Interest

No conflict of interest.

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